

In Vitro and *In Vivo* Biofilm Wound Models and Their Application

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Abstract

Chronic wounds are wounds which are detained in one or more phases of normal wound healing. It is estimated that 1–2 % of the population of developed countries will experience a chronic wound during their lifetime and this number is expected to increase given the growing world population, increase in age, body mass index and associated diseases such as diabetes and cardiovascular diseases. Although several factors contribute to wound healing, presence of bacterial biofilms significantly affects healing and success of wound treatment. This indicates that wound-care therapies should be directed towards targeting biofilms within chronic wounds. Despite this, the role of biofilms in chronic wound pathogenesis and the effect of wound-care therapies against biofilms within wounds are not well understood. In order to address these issues, appropriate biofilm models are necessary. To this end, several model systems mimicking the conditions observed in a biofilm infected chronic wound have been developed. In this review we present an overview of these different *in vitro* and *in vivo* biofilm wound model systems and discuss their advantages and disadvantages.

Keyword

Chronic wounds • Biofilms • *in vitro* wound biofilm models

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1 Introduction

Chronic wounds are wounds which are detained in one or more phases of normal wound healing (Lazarus et al. 1994). Diabetic, arterial, venous and pressure ulcers constitute the majority of these wounds. Chronic wounds affect between two and seven million of patients annually with

treatment costs rising up to several billions of dollars annually (Sen et al. 2009). It has been estimated that 1–2 % of the population of developed countries will experience a chronic wound during their lifetime and this number is expected to increase given the growing world population, increase in age, body mass index and associated diseases such as diabetes and cardiovascular diseases (Gottrup 2004). Although several factors contribute to wound healing, bacterial infections can significantly affect healing and success of wound treatment (Robson 1997; White and Cutting 2006; Wolcott et al. 2010b). The moist environment and the constant supply of nutrients within the wound represent the ideal environment for bacterial growth. These bacteria can come from different exogenous (e.g. soil and water) as well as endogenous (e.g. skin, saliva, urine, faeces) sources. However, the biodiversity is suggested to be relatively low and *Staphylococcus aureus* and *Pseudomonas aeruginosa* seem to predominate in chronic wounds (Bowler 1998; Fazli et al. 2009; Gjodsbol et al. 2006; Kirketerp-Møller et al. 2008; Rao and Lipsky 2007; Rhoads et al. 2012).

Increasing evidence suggest that these bacteria reside within biofilms in these wounds (Bjarnsholt et al. 2008; Burmølle et al. 2010; Church et al. 2006; James et al. 2008). Biofilms are sessile communities characterized by microbial cells that are irreversibly attached to a substratum and/or to each other and are embedded in a self-produced matrix of extracellular polymeric substances and exhibit an altered phenotype compared to planktonic cells (Costerton et al. 1999). Bacteria living in these biofilms are well protected against antimicrobial agents and host defenses and are for that reason extremely difficult to eradicate (Fux et al. 2003; Bjarnsholt et al. 2008). Recent studies have shown that the major reason for the failure of wound treatment and the shift from acute towards a chronic wound is the presence of bacterial biofilms within the wounds (Harrison-Balestra et al. 2003; Bjarnsholt et al. 2008; Davis et al. 2008; Kirketerp-Møller 2008; Kirketerp-Møller and Gottrup 2009). Only 6 % of acute wounds contained biofilms while this was between

60 and 80 % for chronic wounds (James et al. 2008). In addition, in a study of Dowd et al. (2009) only wounds without detectable biofilm showed signs of wound healing. This indicates that wound-care therapies should be directed towards targeting biofilms within chronic wounds. Despite this, the role of biofilms in chronic wound pathogenesis and the effect of wound-care therapies against these biofilms are not well understood. In order to address these issues, appropriate biofilm models are necessary. To this end, several model systems mimicking the conditions observed in a biofilm infected chronic wound have been developed. In this review we present an overview of these different *in vitro* and *in vivo* biofilm wound model systems and discuss their advantages and disadvantages.

2 Static *In Vitro* Wound Models

Different biofilm models have been used to evaluate the effect of antimicrobial agents on biofilms (see Coenye and Nelis 2010 for a general overview of biofilm model systems). These “general purpose models” can be used to evaluate the efficacy of wound care products or to evaluate biofilm formation of wound isolates. However, most of these *in vitro* models do not reflect the micro environmental conditions found in the wound bed. For this reason, several researchers have made specific adaptations to these general static biofilm models trying to better mimic wound-like environments in an easy-to-handle *in vitro* setting. For example, static biofilm models were developed in which biofilms were grown on agar, poloxamer gels or cellulose matrixes placed in petri-dishes (Clutterbuck et al. 2007; Percival et al. 2007; Hammond et al. 2011; Merritt et al. 2011; Kim and Izadjoo 2015) (Table 1). Although poloxamer gels are polysaccharides, bacterial cultures growing on this substrate mimic many of the properties of biofilm-grown bacteria. Similarly, the permeable nature of cellulose disks allows diffusion of nutrients to the bacteria on the disk, just as nutrients are supplied to biofilms in a wound. As such, both set-ups have been used to evaluate

Table 1 Overview of different static *in vitro* chronic wound models

Characteristics	Percival et al. (2007)	Sun et al. (2008)	Werthén et al. (2010)	Kostenko et al. (2010)	Hammond et al. (2011)	Kucera et al. (2014)
Designation	Poloxamer model	LBCW	Collagen wound model	MBEC wound model	Cellulose agar model	Artificial wound bed model
Use of a wound like surface	No	No/Yes	Yes	Yes	No	No
	(Poloxamer gel)	(plastic tip, silicone disk or host-derived matrix)	(Collagen matrix)	(Serum coated pegs)	(Cellulose disks)	(Plastic)
Use of a wound like medium	No	Yes	Yes	No	No	Yes
	(MH-agar)	(Bolton Broth, 50 % bovine plasma, 5 % freeze-thawed lacked horse-blood)	(SWF: 50 % fetal calf serum and 50 % physiological NaCl in 0.1 % Pepton (PW) or a 1:1 TSB-SWF solution)	(TSB)	(LB-agar)	(Bolton Broth, 1 % gelatine, 50 % porcine plasma, 5 % freeze-thawed porcine erythrocytes or Bolton broth +1 % gelatine +1.2 % agar)
Air-liquid interface	Yes	No	Yes	No	Yes	Yes
Flow present	No	No	No	No	No	No
Inoculum	10 ⁵ –10 ⁶ CFU	10 ⁴ CFU	10 ⁴ –10 ⁵ CFU	10 ⁷ CFU/ml	10 ² –10 ⁴ CFU	10 ⁴ CFU
Incubation temp	25–35 °C	37 °C	35–37 °C	37 °C	37 °C	37 °C

the effect of silver containing dressings (Percival et al. 2007, 2011), antibiotic ointments and agents (Clutterbuck et al. 2007; Hammond et al. 2011; Miller et al. 2014) and garlic (Nidadavolu et al. 2012). In addition, Kostenko et al. (2010) evaluated the efficacy of silver containing dressings using an MBEC (“Minimal biofilm eradication concentration”) device. This set-up allows a non-destructive transfer of the biofilms into fresh medium. Biofilms in this device grow on pegs attached to the lid of the device which were coated with serum. Although, most of these general batch culture models have the advantage of being simple and allowing high throughput screening in a cost-effective manner and although some adaptations have been made to better reflect a wound environment, none of them convincingly mimics the conditions observed in an *in vivo* wound.

2.1 Lubbock Chronic Wound Biofilm Model and Derived Models

The first chronic wound model that truly attempted to mimic wound like conditions was developed at the medical biofilm research institute in Lubbock (Texas, US) and was therefore named the “Lubbock chronic wound biofilm model (LCWB)” (Table 1) (Sun et al. 2008). This model allowed the rapid (24 h) cultivation of a robust multispecies biofilm in which *P. aeruginosa*, *S. aureus* and *Enterococcus faecalis* are present in roughly equal ratios. These bacteria were chosen since they are often isolated from and co-occur in chronic wounds (Sun et al. 2008; Gjodsbol et al. 2006). However, the LCWB allows growth of several Gram negative and Gram positive bacteria, aerobes as well

as anaerobes (DeLeon et al. 2014; Dalton et al. 2011). An inoculum of 10^4 cells was used to represent a normal microbial load of a wound prior to infection. Biofilms are grown in a medium consisting of a chopped meat-based medium (Bolton broth) with 50 % heparinized bovine plasma and 5 % freeze-thaw laked horse red blood cells. As such the medium presents the major host factors (e.g. damaged tissue, red blood cells and plasma) found in a typical wound bed. A major downside of this model is the fact that biofilms are formed using a plastic tip or silicone disks as a substrate, which does not reflect a wound-like surface (Sun et al. 2008; Brackman et al. 2011). However, it was recently shown that the medium coagulates into a jelly-like mass when a coagulase-positive bacterial species is used (such as *S. aureus*). *S. aureus* secretes staphylocoagulase which binds to prothrombin, forming a complex which converts soluble fibrinogen to insoluble fibrin. As such there is no need for using an artificial surface since a host-derived matrix is formed which can serve as a scaffold to which bacteria can adhere and form biofilms (DeLeon et al. 2014). Another encouraging aspect of this *in vitro* model is the morphological similarity that is being observed, both with the naked eye as well as on electron micrographs, between biofilms grown in the model and biofilms on actual chronic wounds. As such, this model was shown to be a realistic *in vitro* model which is easy to handle and allows rapid growth and maturation of a multispecies biofilm in a cost effective manner. For this reason, the LCWB has been used extensively to study interspecies interactions (Dalton et al. 2011; DeLeon et al. 2014) and to assess the effect of antibiofilm compounds, antimicrobial agents, hydrogels, functionalized gauzes and dressings against both single species biofilms and polymicrobial communities (Garcia-Fernandez et al. 2013; Luna-straffon et al. 2014; Douglas et al. 2014; Sun et al. 2009; Dowd et al. 2009; Brackman et al. 2011).

Since the first publication, several research groups have made adaptations to the LCBW model to address specific needs. The evaluation of the effect is typically based on quantification

of the number of biofilm cells by plating or by using quantitative qPCR methods, making it less suitable for screening large amounts of compounds. Recently, the LCWB was modified for high throughput testing to address this need (Brackman et al. 2013). A good correlation was observed between the fluorescence from a fluorescent *S. aureus* strain and the number of biofilm cells present after treatment (Brackman et al. 2013).

The LCWB model is often used to obtain polymicrobial wound-like biofilms which are then transplanted into other *in vitro* and/or *in vivo* models of skin infection. For example, Dalton et al. (2011) successfully transplanted a biofilm cultured in the LCWB model into a murine skin wound to induce *in vivo* formation of wound biofilms. In addition, Kucera et al. (2014) developed an artificial wound bed model for assessment of solid antimicrobial dressings based on the LCBW model. In brief, the biofilm was pre-cultured using the LCBW set-up with some modifications and amendments. These included the addition of gelatin to the wound medium and the use of porcine plasma and freeze-thaw laked porcine erythrocytes instead of bovine plasma and horse blood. This pre-cultured biofilm was then transferred onto an artificial wound bed. This artificial wound bed consists of a two-layer nutrient medium composed of Bolton Broth supplemented with 1 % gelatin (w/v) and 1.2 % agar (w/v). The use of the artificial wound bed in the model enables to mimic the situation in chronic infected wounds where the biofilm is only in partial contact with the wound dressing. The modified set-up also incorporates an air-liquid interface feature which is usually present in wound biofilms.

2.2 Collagen-Based *In Vitro* Wound Models

In *in vitro* models, biofilms are often formed on solid, artificial surfaces. This makes it difficult to correlate the *in vitro* results with *in vivo* observations, since the full contribution of the surface to biofilm formation and biofilm

persistence is often unknown. In addition, bacteria in wounds are often not attached to well-defined solid surfaces, but instead reside in the wound bed. For this reason, a model system in which sessile bacteria are aggregated in the absence of a solid surface would mimic the conditions in the wound more closely. To address this issue, Werthén et al. (2010) developed an *in vitro* wound model in which biofilms can develop in the presence of simulated wound fluid (containing 50 % fetal calf serum and 50 % physiological saline in 0.1 % peptone) and a matrix of polymerized rat-tail collagen type I but in the absence of a solid surface (Table 1). Both *P. aeruginosa* and *S. aureus* formed aggregates, surrounded by self-produced polysaccharide matrix within the collagen matrix (Werthén et al. 2010). In addition, biofilms formed in this model were structurally similar to biofilms observed *in vivo*, suggesting the presence of a “wound-like” environment (Werthén et al. 2010). The deep penetration of *P. aeruginosa* biofilms and the more surface-oriented biofilms of *S. aureus* observed in this model resembled other *ex vivo* observations (Kirketerp-Møller et al. 2008). For this reason, this model was used to better predict the *in vivo* antimicrobial activity of antibiotics and silver-containing wound-dressings in several studies (Brackman et al. 2011; Hakonen et al. 2014).

3 In Vitro Chronic Wound Models with Liquid Flow

Although the above mentioned biofilm models aim to mimic *in vivo* wound-like environments, all of them are based on closed and therefore accumulative batch culture systems. For this reason, some argue that it is unlikely that they will fully represent the true dynamic state of the wound environment. To address this issue several *in vitro* wound models were developed in which a fluid flow is present and/or in which the biofilm is exposed to shear stress (Thorn and Greenman 2009; Lipp et al. 2010; Hill et al. 2010) (Table 2). The *in vitro* flat-bed perfusion model (Thorn and Greenman 2009),

developed based on previously described static models (Greenman et al. 2006; Thorn et al. 2007) addresses this issue. This model consists of autoclavable removable cassettes containing microscope slides on which 1 cm² cellulose matrices are placed. A hyperdermic needle, linked to a peristaltic pump was used to perfuse growth medium through the removable cassettes. The medium consists of 0.1 % heat-inactivated foetal calf serum (FCS) or 2 % FCS + 0.1 % glucose in phosphate buffered saline depending on whether *P. aeruginosa* or *S. aureus* was used, respectively (Thorn and Greenman 2009). This model can be used to determine the antimicrobial kill kinetic profile of topically applied treatments (Thorn et al. 2009). In addition, a bioluminescent target organism was integrated into the model and shows the feasibility of using light production for real-time monitoring of antimicrobial efficacy (Thorn and Greenman 2009).

Similarly, Lipp et al. (2010) used a colony drip-flow reactor (C/DFR) model to grow *P. aeruginosa* and *S. aureus* biofilms under wound-like conditions. This model was based on characteristics of both the colony biofilm model (Anderl et al. 2000) and the drip-flow reactor (DFR) model (Buckingham-Meyer et al. 2007). In the C/DFR, biofilms are grown on semipermeable membranes which are placed on microscope slides in a DFR apparatus. These membranes are inoculated with approximately 10⁴ CFU of a single species (*P. aeruginosa* or *S. aureus*), left for 30 min to allow drying of the inoculum after which medium (10 % TSB) was pumped through the system (5 ml/h/channel) and biofilms were allowed to form for up to 72 h at room temperature (Lipp et al. 2010). Although initially single species biofilms were grown, growth of a polymicrobial biofilm consisting of bacteria with variable oxygen requirements is possible in this model (Woods et al. 2012). Interesting is the fact that growth of a strict anaerobe (*C. perfringens*) occurred in a polymicrobial biofilm with *P. aeruginosa* and *S. aureus* in the C/DFR, without establishing an artificial anaerobic environment (Woods et al. 2012). As such this model was used to evaluate the effect of antimicrobial agents (Agostinho et al. 2011) and

Table 2 Overview of different dynamic *in vitro* chronic wound models

Characteristics	Thorn and Greenman (2009)	Lipp et al. (2010)	Hill et al. (2010)	Ngo et al. (2012)	Terry and Neethirajan (2014)
Designation	Flat-bed perfusion model	C/DFR	CDFE	CDC-TNP model	Microfluidic wound model
Use of a wound like surface	No (Cellulose matrix)	No (Absorbant pad)	Unclear (not disclosed)	No (Borosilicate or Teflon)	Yes (Collagen)
Use of a wound like medium	Yes (Foetal calf serum (FCS) or 2 % FCS + 0.1 % glucose in PBS)	No (10 % TSB)	No (TSB or BM)	No (TSB or 10 % TSB)	No (TSB + 1 % glucose)
Air-liquid interface	Yes	Yes	Partly ^a	Partly ^a	Partly ^a
Flow present	Yes (1 ml/h)	Yes (5 ml/h)	Yes (30 ml/h)	Yes (11.7 ml/min–40 ml/h)	Yes (100–200 µl/h)
Inoculum	10 ⁵ CFU	10 ⁴ CFU	ND	ND	ND
Incubation temp	37 °C	RT (21.5 °C)	37 °C	30–37 °C	35 °C

^aAn air-liquid interface can be present at different stages (e.g. attachment step, biofilm formation step, evaluation of antibacterial therapies), but not during the entire experiment

ND specific number of cells is not disclosed

wound dressings (Lipp et al. 2010) against mono- and three-species biofilms (Woods et al. 2012).

Recently two different models were developed in which biofilms were first grown in a flow-displacement model and then transferred to an adapted novel *in vitro* wound-like set-up (Ngo et al. 2012; Hill et al. 2010; Malic et al. 2011). These two models are the constant depth film fermenter (CDFE) and the Centers for Disease Control (CDC) biofilm reactor. Both models allow the generation of identical, multiple biofilms simultaneously and allow to vary key parameters including nutrient source, temperature, oxygen availability and substrata (Pratten and Wilson 1999). The reproducibility of identical biofilms, the possibility to image biofilms in three-dimensions and in real-time makes these models interesting starting points to make biofilms which can be implemented in other models.

The CDFE consists of a glass chamber housing a rotating stainless steel disc in which a total of 15 sampling pans, each containing five plugs, are placed. The disc is placed at a set depth and rotates while a scraper plate aids in the

distribution of medium across the plugs and maintains a constant depth of the biofilm by removing biofilm cells growing higher. Similarly, the CDC reactor consists of a glass vessel with eight removable polypropylene rods, each holding three removable coupons on which biofilms can form (Donlan et al. 2004). These are oriented in such a way that the coupon is perpendicular to the rotating baffle (Buckingham-Meyer et al. 2007). The glass chamber of both models contains both entry and exit ports allowing a continuous flow of fresh medium through the system. Hill et al. (2010) used a constant depth film fermenter (CDFE) to form multispecies biofilms consisting of wound isolates. In brief, biofilms were grown at 37 °C on plug inserts into the CDFE placed at a 400 µm depth. BM (Hill et al. 2010) or BHI (Malic et al. 2011) medium was pumped through the system at a rate of 30 ml/h. After biofilm formation, biofilms were transferred to a moistened dressing in a sterile petridish (Hill et al. 2010). This set-up has been used to evaluate the effect of different antibiotics, commercial dressings and anti-biofilm compounds (Hill et al. 2010). In addition,

this model was further used to evaluate co-aggregation, synergy and antagonism between bacteria isolated from different types of wounds (Hill et al. 2010; Malic et al. 2011). Similarly, a CDC biofilm reactor was used to form single species biofilms which are then placed in an *in vitro* wound model (Ngo et al. 2012; Valente et al. 2014). In brief, biofilms were grown in a CDC biofilm reactor on borosilicate coupons at 30 °C using Trypton soy broth which was supplied at a rate of 11.7 ml/min. After biofilm formation, coupons were taken out of the CDC and embedded into an agar base representing a low nutrient and moist organic wound surface. A major difference with the CDFF set-up was that a constant flow of 1 % TSB at 40 ml/h was provided across the agar surface by an intravenous infusion (Ngo et al. 2012). This model is mainly used to evaluate the effect of negative pressure by itself or in combination with silver impregnated foam dressings on wound biofilms (Ngo et al. 2012; Valente et al. 2014).

4 Microfluidic Wound Models

A major downside of most of the above mentioned methods is the need for relatively large amounts of test-compounds when evaluating their efficacy in these models. Microfluidic-based wound models can overcome this drawback (Zhang et al. 2013). Microfluidic technology is a relatively new field that is already applied to study biofilm growth in a confined space (e.g. mimicking biofilm growth in a blood vessel) (Sato et al. 2014), to study antimicrobial resistance in biofilms by creating dynamic concentration gradients and/or to study spatial and temporal growth of micro-organisms as well as motility and chemotaxis in biofilms (Kim et al. 2012; Halder et al. 2013). Although differences between microfluidic devices exist, the channels are typically 50–500 µm wide, 30–500 µm deep and 1–40 mm in length. In addition, flow rates are usually low (0.1–50 µl/min) (Coenye and Nelis 2010). Recently, a “microfluidic wound model” was described which is easy to use, relatively cheap and small

(Terry and Neethirajan 2014) (Table 2). In order to better mimic wound like surfaces, the channels were coated with rat tail collagen type I before bacteria were pumped through the system (Terry and Neethirajan 2014; Chen et al. 2014).

Although microfluidic wound models have several advantages compared to other models (e.g. use of a flow while only small amounts of test product are needed) there is still room for improvement on different other levels (e.g. use of more relevant media, surfaces and mixed biofilms). In this view it is interesting to note that microfluidic co-culture models are being developed in which biofilms can develop in the presence of an epithelial cell monolayer (Kim et al. 2010a, b; Zhang et al. 2013). Recently, Zhang et al. (2013) developed a microfluidic wound-scratch model system to investigate cell migration and proliferation. Although this model was not published in the context of infected wound biofilms, it displays the possibility of upgrading existing models to better emulate the conditions observed in an infected *in vivo* chronic wound.

5 Issues with the *In Vitro* Wound Models

Although all of the above mentioned *in vitro* models address specific aspects of wound biofilms, they all are prone to limitations (Tables 1 and 2). First of all, although some models display flexibility in the use of different bacterial species and/or mixed biofilm communities, most of the *in vitro* wound models only rely on the use of a single bacterial species. As such it is unclear whether these models would allow the incorporation of a biofilm consisting of different bacterial species. Dominant single species biofilm aggregates of *S. aureus* and *P. aeruginosa* are observed in infected chronic wounds and the outcome of wound healing can be correlated with the presence of a specific species. However, infected chronic wounds are often polymicrobial in nature, despite the fact that bacterial diversity is generally low (Robson 1997; Rao and Lipsky 2007; Colsky et al. 1998;

Gjodsbol et al. 2006; Fazli et al. 2009; Rhoads et al. 2012). For this reason, increasing the complexity of the model by adding multiple species could make the model system more relevant.

A second issue is the temperature used. Most of these biofilms are formed and maintained at 37 °C which reflects core body temperature. However, although skin temperature can be different due to variability between persons and body location, temperature of trauma wounds and wound bed temperature of chronic leg ulcers ranges between 25–37 °C and 24–26 °C, respectively (Fierheller and Sibbald 2010; Romanelli et al. 2002). This temperature is significantly lower than what is often used in the different models, which would indicate that conducting experiments at lower temperatures would better reflect the chronic wound bed temperature.

A wide range of different inocula are also being used in these models. These inocula range between 10^2 and 10^8 CFU. It is generally accepted that infected chronic wounds contain more than 10^5 bacteria per gram of tissue (Robson 1997; Bowler 2003). Although it is highly questionable that high bioburden levels are present at the start of infection under proper standard care conditions, models applying these higher inocula might be representative for heavily infected wounds or wounds inflicted under conditions where proper wound-care is not directly possible. In addition, lower inocula can be used for investigating biofilm development from the start of an infection. As such the inoculum used, should depend on the question that needs to be answered and it should be clear whether different inocula can be used in the different model systems.

Thirdly, the surface and media used in some models often do not reflect the nutritional conditions which bacteria would find in wound beds. Surfaces such as glass, silicone and plastics do not resemble the surfaces on which biofilms are formed in real wounds. In addition, although some artificial surfaces (such as poloxamer gels and cellulose disks) do possess some wound-like features, it remains questionable whether these would evoke similar responses in bacterial gene expression, biofilm formation and resistance to

therapy as to biofilms grown on biotic surfaces. As such, most of these *in vitro* models do not take into account the role that dermal substrates can play on bacterial attachment, nutrition, biofilm shape and resistance and for this reason these models could be adapted at the level of the surfaces used in order to better mimic wound like conditions. Similarly, general media such as TSB or LB support the growth of a wide variety of microorganisms, but they do not contain many of the components which are present in wound exudates. Specific media such as the simulated wound fluid (Werthén et al. 2010) or media containing plasma, serum, blood cells and/or heparin likely better reflect nutritional conditions observed in wounds. However, to date there is no standardized nutrient medium to replicate wound exudates under *in vitro* conditions and the composition of wound fluid and wound exudates can be highly variable depending individual, type of wounds and wound healing stadium (Trengeve et al. 1996, 1999; Cutting 2003; Eming et al. 2010). It thus remains difficult to really define which media would reflect wound conditions best.

Finally, as crucial is the expected geometry of how nutrients are applied to the wound biofilm. Although this might vary depending on the wound type and amount of exudate produced, nutrients generally originate from the host tissue at the bottom of the biofilm, while oxygen is usually supplied from the top of the biofilm at the air-liquid/surface interface. In addition, the physical aspect of a low fluid shear might be important in specific wound types. Although most of the *in vitro* wound model systems take into account one or more of these aspects in order to mimic *in vivo* wounds, none of them take into account all these aspects (Tables 1 and 2).

6 Cell-Based Wound Models

Implementing skin as a substrate for attachment and as the primary source of nutrition for microbial biofilm cells would allow the formation of biofilms under conditions which would more closely resemble the *in vivo* situation. For this

reason, several more advanced cell-based wound models were developed in which porcine skin explants (Yang et al. 2013; Phillips et al. 2013; Wolcott et al. 2010a), two-dimensional cell monolayers or three-dimensional tissue-engineered human skin equivalents (TE-HSE) (Haisma et al. 2013; Charles et al. 2009) were used as a substrate for biofilm development.

Given the fact that pig skin and human skin have striking similarities in structure (Summerfield et al. 2014), cell-based wound models using porcine skin explants have been used to study molecular characteristics of biofilms attaching to skin (Yang et al. 2013), assess the efficacy of antimicrobial agents and antimicrobial wound care dressings against *P. aeruginosa* and *S. aureus* biofilms and assess the effect of negative pressure wound therapy with instillation of antimicrobial solutions against *P. aeruginosa* biofilms (Phillips et al. 2010, 2013). A main disadvantage is that significant differences still exist between human and animal skin at the level of immunological responses (Summerfield et al. 2014). Despite this, human explants have rarely been used since it would be difficult to standardize and reproduce results obtained in such models. The development of reconstituted human tissue models using two-dimensional cell monolayers or three-dimensional tissue-engineered human skin equivalents would overcome this issue. Although monolayer cultured cells are often used, such studies do not accurately reflect the behavior, pathophysiology, or microenvironment of skin *in vivo* (Welss et al. 2004). Cells in monolayer culture are in isolation and for this reason do not take into account that bacteria invade and interact with different cell types in a complex three-dimensional solid structure. For this reason, three-dimensional systems would better mimic *in vivo* infections. Tissue-engineered human skin equivalents (HSE) are three-dimensional systems that mimic the native skin to a high degree (Welss et al. 2004). Although different HSE are described in literature, they are typically generated by culturing primary keratinocytes and dermal fibroblasts at the air-liquid interface of cell-free matrices

(e.g. filters, collagen gels or decellularized dermal scaffolds such as de-epidermized dermis). The cells will proliferate, migrate and differentiate during peridermal development resulting in skin equivalents that usually contain all layers of the native epidermis and/ or dermis (El Ghalbzouri et al. 2004, 2008; Charles et al. 2009; Welss et al. 2004; Torkian et al. 2004). In addition, several HSE are commercially available. Epiderm-FT (MatTek, MA, US) is a multilayered highly differentiated skin model consisting of human-derived keratinocytes and fibroblasts in cell culture inserts. Apligraf is a tissue engineered skin equivalent which consists of a lower dermal layer (collagen and human fibroblasts) and an upper epidermal layer (human keratinocytes which can differentiate). In addition, reconstructed human epidermis (RHE, Skinethic, Lyon, France) consists of normal human keratinocytes cultured on an inert polycarbonate filter at the air-liquid interface, in a chemically defined medium. The HSE is typically wounded using a biopsy punch or a device heated or cooled with boiling water or liquid nitrogen, respectively, prior to infection (El Ghalbzouri et al. 2004; Haisma et al. 2013; Shepherd et al. 2009). Others have demonstrated that bacteria can colonize HSE and trigger the expression of pro-inflammatory cytokines/chemokines by the underlying cells (Holland et al. 2008, 2009; De Breij et al. 2012; Haisma et al. 2013; Kirker et al. 2009, 2012; Charles et al. 2009). In addition, HSE wound models were used to assess the antimicrobial activity of different agents and plasma against bacterial biofilms under wound like conditions (Haisma et al. 2013; Shepherd et al. 2009; Brackman et al. 2011).

Recently, Bellas et al. (2012) developed a full-thickness skin equivalent which included epidermis, dermis, and hypodermis. This model would serve as a more physiological relevant system that would likely sustain physiological function for more extended time periods in ways that would permit both acute, short-term, and chronic, long-term studies of skin development and pathogenesis. In addition, the morphology and organization of the tri-layer skin model

would allow secretion of appropriate levels of cytokines and mimic the full spectrum of biological functions of skin. The cell-based models have the advantage that they are histologically similar to human skin and thereby provide a controlled environment similar to the one encountered in *in vivo* wounds. However, unlike human skin, these usually do not contain Langerhans' cells, macrophages, lymphocytes or other structures such as blood cells, hair follicles or sweat glands.

7 In Vivo Wound Model Systems

To address the above mentioned issues, several *in vivo* wound models were developed, each with their own strengths and weaknesses (Seth et al. 2012). These animal models are needed since it is virtually impossible to study the development of chronic wound in humans. This is due to ethical concerns, but also due to the fact that the chronic wound is often already present when patients arrive in the clinic. In addition, when these wounds are investigated, this will only be observational thereby lacking the experimental and causative data necessary to fully investigate the role of biofilms and interplay with therapeutically agents (Seth et al. 2012).

One of the first studied *in vivo* models of wound infections relied on the use of *Drosophila melanogaster* (reviewed by Apidianakis and Rahme 2009). A wound infection in the cuticular epithelium and underlying muscle is established in this model by using a thoracic or abdominal pin prick which was dipped in a bacterial suspension. As such, this model was used to study host responses to wound infection by different microbes. Despite being often used, the translation of results obtained in an invertebrate pin-prick wound system to what could be expected in human wounds is questionable. For this reason, mostly vertebrate animals such as mice, rats, pigs and rabbits are used in *in vivo* wound model systems (Table 3). Next to the type and breed of animal used, these models mainly differ in the mechanisms by which wounds are inflicted, how wounds (and infection) is being

maintained during the experiment, on the inoculum size and whether or not different bacterial species were shown to be capable of infecting the host under the given circumstances.

Akiyama et al. (1996) described biofilm formation of *S. aureus* in incisional wounds of mice and this model was later on used to evaluate topical treatment on biofilm susceptibility (Akiyama et al. 2002). Similarly, Rumbaugh et al. (1999) and later on Rashid et al. (2000) examined the role of different genes (including quorum sensing genes) on *P. aeruginosa* virulence in a burn wound mouse infection model. However, the effect of biofilm infection on the global wound healing process or host responses was not assessed. Similarly, several other murine infection models are published in which wounds are caused by thermal injury (Trøstrup et al. 2013; Nichols et al. 2013). Although these models can be useful to study burn wound infections, they do not always represent conditions found in chronic wounds which not originated from burns. For this reason several other models have focused on inflicting wounds by other manners such as biopsy punch (Thompson et al. 2014; Schierle et al. 2009; Zhao et al. 2010; Petreaca et al. 2012; Gurjala et al. 2011), surgical incision (Ermolaeva et al. 2011; Asada et al. 2012; Watters et al. 2014) or by means of sanding (Roche et al. 2012a, b) or pressure (Nakagami et al. 2008). Besides inflicting a wound, maintaining a biofilm infection within these models for a certain amount of time remains challenging. For this reason several models rely on specific preconditioned animals (e.g. mutant breeds or induction of specific pathogenesis such as diabetes), the pre-formation of the biofilm under *in vitro* conditions before the biofilm is applied to the wound bed and/or placement of dressing materials to maintain a moist environment (Table 3). Most of the rodent models also ignore the fact that contracture should be minimized in these models. By minimizing contractures, e.g. by placement of silicone rings around the wound bed, wounds are allowed to heal by new tissue ingrowth, more akin to human wounds, as opposed to myofibroblast-mediated

Table 3 Overview of different *in vivo* chronic wound models

Animals	Wound type	Wound location	Wound maintenance	inoculum	Single or mixed species biofilm	Reference
Murine models						
Ddy mice	Cut wounds	Back	– ^a	3.6 × 10 ⁶ CFU/ml	Single (<i>S. aureus</i>)	Akiyama et al. (1996), (2002)
Swiss Webster mice	Thermal injury (90 °C water) (15 % t.b.i.)	Back	– ^a	10 ² CFU	Single (<i>P. aeruginosa</i>)	Rumbaugh et al. (1999), Rashid et al. (2000)
Swiss Webster mice	Surgical excision wound (1.5 cm ²)	Dorsal	Opsite dressing	10 ⁴ CFU	Single (<i>P. aeruginosa</i> and <i>S. aureus</i>)	Watters et al. (2014), Turner et al. (2014)
BalB/c mice	Thermal injury (hot air) (6 % t.b. i.)	Back	Seaweed alginate beads	10 ⁷ CFU/ml	Single (<i>P. aeruginosa</i>)	Wolcott et al. (2010a), Gawande et al. (2014)
C57BL/6 J mice	Thermal injury (10 % t.b.i.) and abrasion injury	Dorsal	Abrasion injury prior to infection	10 ⁶ CFU	Single (<i>P. aeruginosa</i>)	Trøstrup et al. (2013))
Adult male C57Bl6/J mice	Excisional punch wounds	Back	Silicone rings and covered with Tegaderm	Pre-formed biofilm ^b	Single (<i>S. aureus</i> and <i>S. epidermidis</i>)	Nichols et al. 2013
Male SWR/J and male TH mice	Full-thickness dermal wounds (ND)	Dorsal	Silicon splints and tegaderm dressing	10 ⁶ CFU	Single (<i>S. aureus</i>)	Schielle et al. (2009)
Db/db mice	Full-thickness punch wounds	Dorsal	Dressing occlusion	Pre-formed biofilm ^b	Single (<i>P. aeruginosa</i>)	Nguyen et al. (2013)
BALB/c	Biopsy punch	Dorsal	Tegaderm dressing	5 × 10 ⁴ CFU	Single (<i>A. baumannii</i>)	Zhao et al. (2010)
BALB/c mice	Full thickness wound (ND)	Back	Gauze patch	5 × 10 ⁷ CFU	Single (<i>S. aureus</i>)	Thompson et al. (2014)
LIGHT –/– mice	Biopsy punch	Dorsal	tegaderm	10 ⁸ CFU/ml	Single (<i>S. epidermidis</i>)	Simonetti et al. 2008
Mice (type not disclosed)	Wounded by sanding	Back	Moistened bandage	2 × 10 ⁷ CFU	Single (<i>S. aureus</i>)	Petreaca et al. (2012), Dhal et al. (2014)
Adult male Sprague Dawley rats	Surgical incision	Nape (back of the neck)	Cotton pellets	10 ⁸ CFU/ml	Mixed (<i>P. aeruginosa</i> and <i>S. aureus</i>)	Roche et al. (2012a)

(continued)

Table 3 (continued)

Animals	Wound type	Wound location	Wound maintenance	inoculum	Single or mixed species biofilm	Reference
Adult male Sprague Dawley rats	Scissors incision	Flank region	Tegaderm dressing	2×10^9 CFU	Single (<i>P. aeruginosa</i>)	Asada et al. (2012)
male Wistar rats	Pressure-related ischemic wounds	lateroabdominal and dorsal regions	- ^a	10^5 CFU	Single (<i>P. aeruginosa</i>)	Nakagami et al. (2008)
Pig models						
Commercially raised, specific pathogen-free, female Yorkshire-cross pigs	Full thickness trephine (2 cm) wounds	Back	Gauze pad and tegaderm dressing	10^7 – 10^8 CFU	Single (<i>S. aureus</i>)	Roche et al. (2012b)
Young, female, specific pathogen-free pigs	Wounded using a modified electrokeratome set	Back and side	polyurethane film dressing (tegaderm) and self-adherent bandages	10^6 – 10^7 CFU/mL	Single and mixed (<i>P. aeruginosa</i> and <i>S. aureus</i>)	Davis et al. (2001, 2007, 2008), Pechter et al. (2012), Pastar et al. (2013), Nusbaum et al. (2012)
Rabbit models						
New Zealand white rabbits	Full-thickness dermal punch wounds	Ventral side of each ear	Tegaderm dressing	10^6 CFU	Single and mixed (<i>K. pneumoniae</i> , <i>P. aeruginosa</i> and <i>S. aureus</i>)	Gurjala et al. (2011), Seth et al. (2012), Chen et al. (2014), Leung et al. 2014

^aNo specific wound-maintenance strategy mentioned^bPre-formed biofilm. Specific inoculum number not disclosed

ND specific mechanism not disclosed

contraction of the loose rodent skin (Schierle et al. 2009; Nguyen et al. 2013). Additionally, only a limited amount of models study the infection for a longer period of time (Thompson et al. 2014; Roy et al. 2014). Although the use of mice and rats have some advantages over the use of larger animals such as pigs (e.g. ease-of-use, space-limitations, economical and ethical concerns), pigs are preferred for wound healing studies due to higher similarities between porcine and human skin and due to the scale at which wounds can be introduced (Sullivan et al. 2001; Summerfield et al. 2014). In addition, with respect to the translational value, the use of pigs as preclinical model for wound studies is recommended (Gordillo et al. 2013). Recently, an *in vivo* biofilm wound infection model was developed in rabbits (Gurjala et al. 2011). This model was based on the rabbit dermal ulcer model, which is an FDA-recognized model of wound healing which has been used for over two decades (Mustoe et al. 1991; Chen et al. 1999; Said et al. 2005; Mogford et al. 2009). In this model, full-thickness, circular punch-wounds are made in the ears of New Zealand White rabbits down to cartilage, affording a number of important advantages. For example, in contrast to partial-thickness wounds, this removal of dermis more closely models the dermal-loss seen in human chronic wounds. Additionally, the majority of human wounds heal through epithelialization and granulation, in contrast to the contracture-based healing seen in mice (Schierle et al. 2009). The underlying cartilage of the rabbit ear serves as a natural splint, preventing healing by contracture, and thus allowing for accurate quantification of epithelial and granulation tissue formation from the periphery of the wound. Moreover, multiple identical wounds can be made in one animal with contralateral controls, creating a standardized and high-throughput wound model. In contrast to other published models where pre-formed *in vitro* biofilm is directly applied to wounds, these wounds are inoculated with planktonic, free-floating bacteria which more closely represents the seeding mechanism of human chronic wounds, with the wound bed

itself playing a critical role in the transformation of bacteria into the biofilm state (Schultz et al. 2004; Cierny and DiPasquale 2006). Although different *in vivo* models exist, the clinical relevance of these models is still being argued (Seth et al. 2012). These aspects should be addressed in the future.

8 Concluding Remarks

Investigating wound infections and development of novel therapeutic agents targeting these types of infections require the existence of appropriate models. As discussed in this review, several *in vitro* and *in vivo* wound model systems have been described, each with their specific strengths and weaknesses and addressing different aspects of wound biofilms. As such, researchers should select a model by measuring out these differences against the questions that they are hoping to answer using these models. However, due to the complexity of wound healing, extrapolation of results from *in vitro* biofilm studies to the clinic will always remain challenging. Only animal models can take into account factors such as interplay of immune responses and wound bed components. In addition, *in vivo* animal models are necessary, since it is virtually impossible to study the development of chronic wound in humans. For this reason, there is a wide consensus that there is a high need for not only conducting these experiments, but also for a further development and improvement of the existing models both *in vitro* as well as *in vivo*. These modifications, including the introduction of polymicrobial biofilms, more relevant media and surfaces, would possibly lead to models which are truly capable of evaluating therapies under *in vitro* and *in vivo* settings. In addition, better models would eventually lead to studies on biochemical pathways (e.g. by use of mutants), host response to infection and on the interplay between different therapeutically agents and the biofilms which would better reflect reality. This would ultimately improve our understanding of why chronic wounds develop and why they are being maintained and altogether these insights

could possibly lead to better therapies addressing the issue of chronic wound infections in the clinic in the future.

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